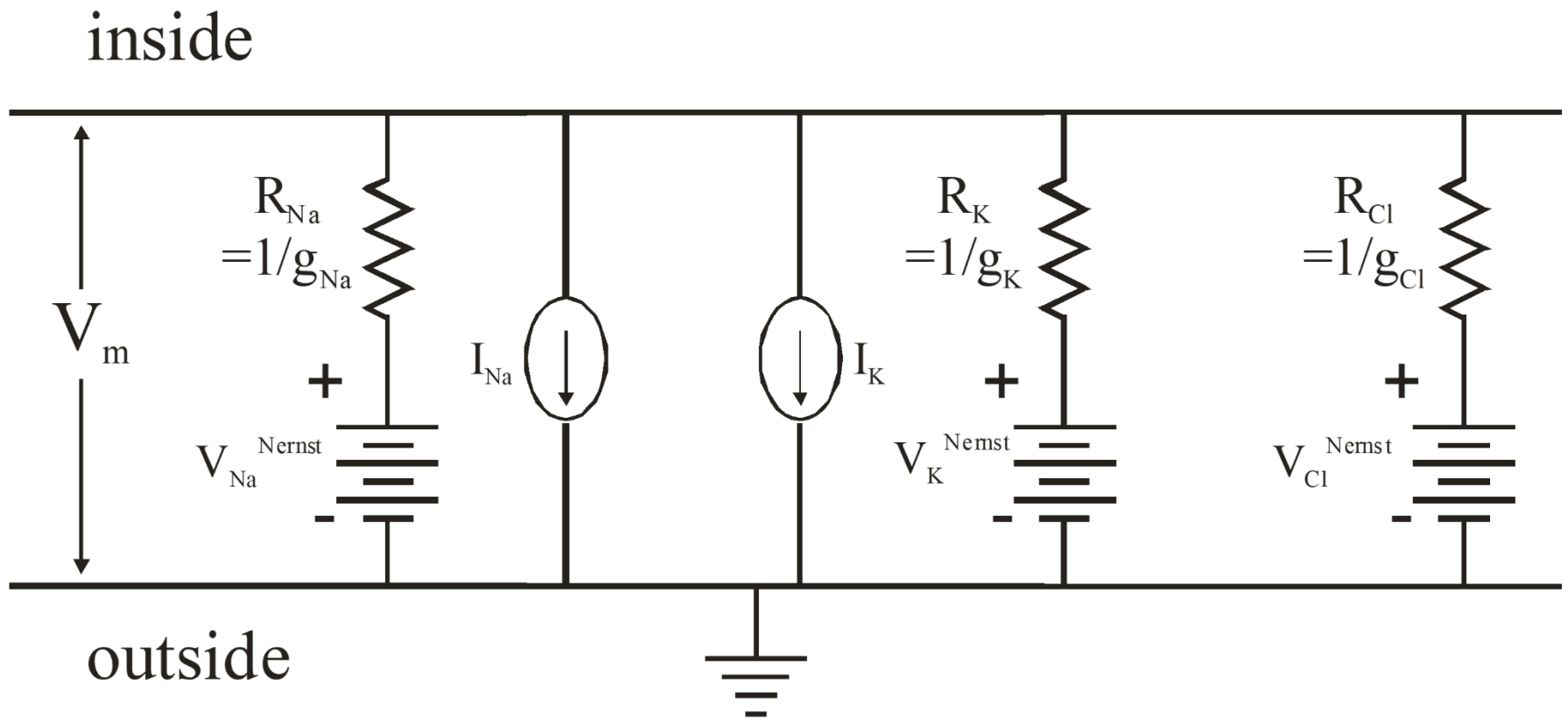


A detailed illustration of a neural network. Numerous neurons are shown, each with a central cell body (soma) and multiple branching processes (dendrites and axons). The neurons are rendered in a reddish-brown color. Several points along the axons and at the cell bodies are highlighted with bright, glowing orange and yellow light, representing the propagation of action potentials. The background is a soft gradient of purple and blue.

# Active membranes and action potentials

- B&B, chapter 7
- Nelson, chapter 12
- K&S, chapter 2



$$V_i^{\text{Nernst}} = -\frac{k_B T}{n_i q} \ln \left( \frac{C_{i,\text{int}}}{C_{i,\text{ext}}} \right)$$

$$j_{q,i}^{\text{ohmic}} = n_i q j_i^{\text{ohmic}} = (\Delta V - V_i^{\text{Nernst}}) g_i$$

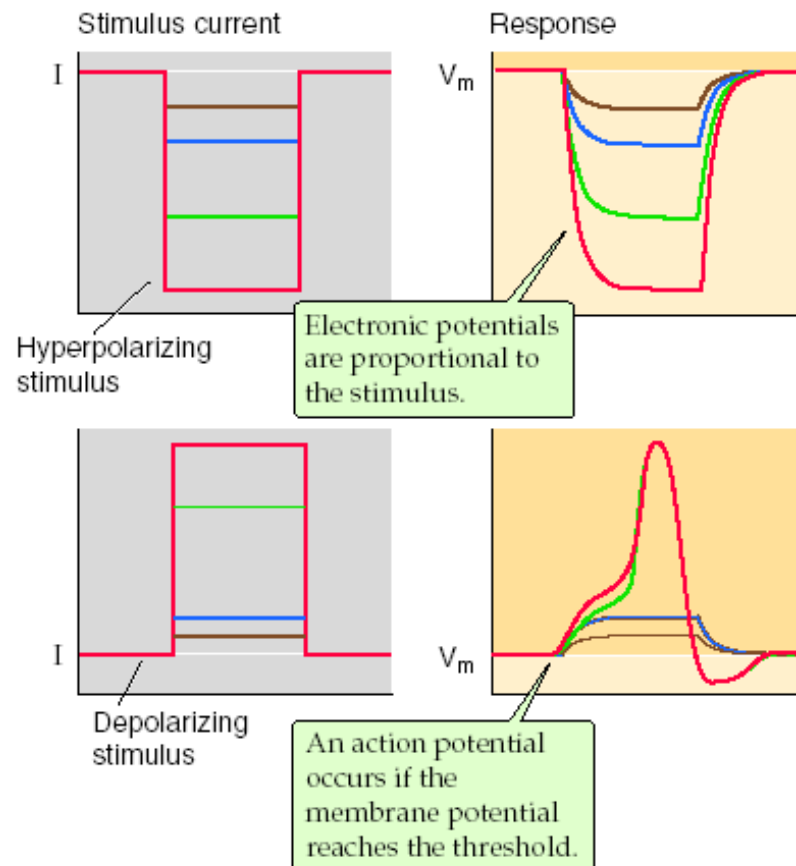
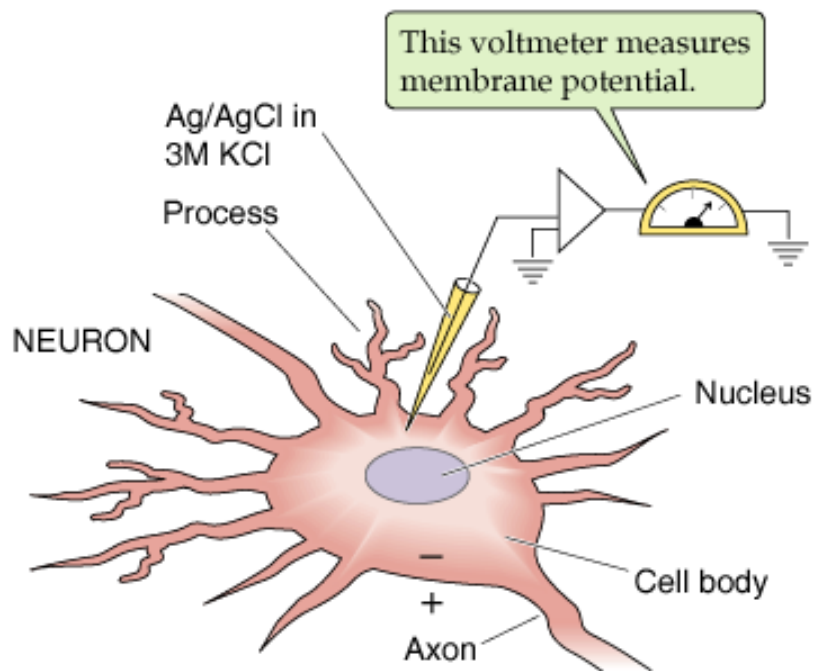
$q$  = charge of electron,  $1.6\text{E-}19$  C

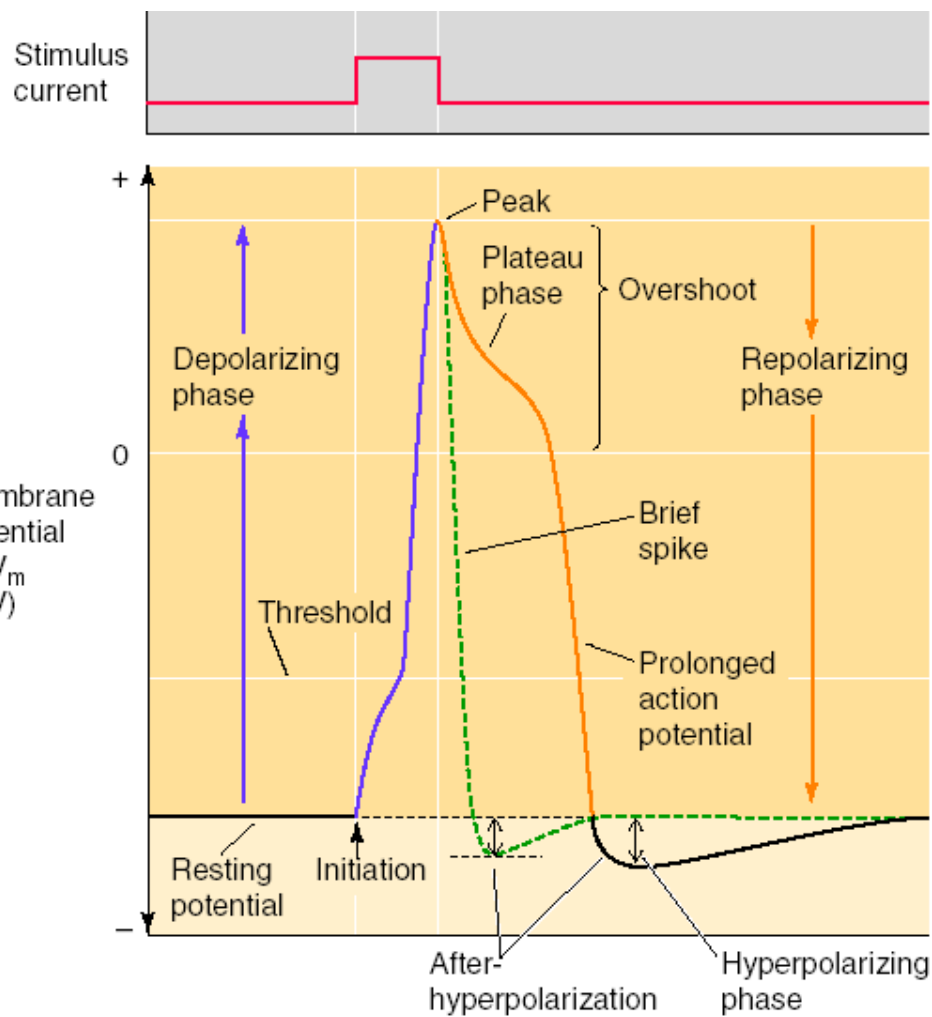
$n_i$  = number of charges on ion

$j_{q,i}$  = current across membrane

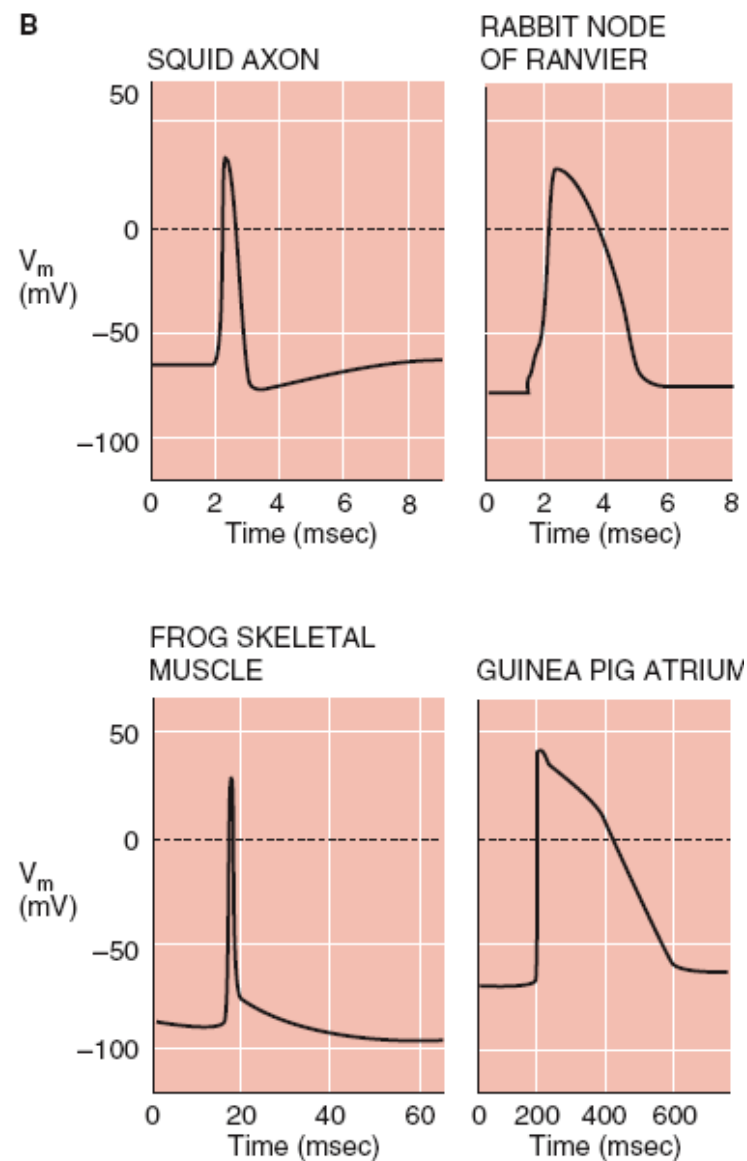
$j_i$  = ion flow across membrane

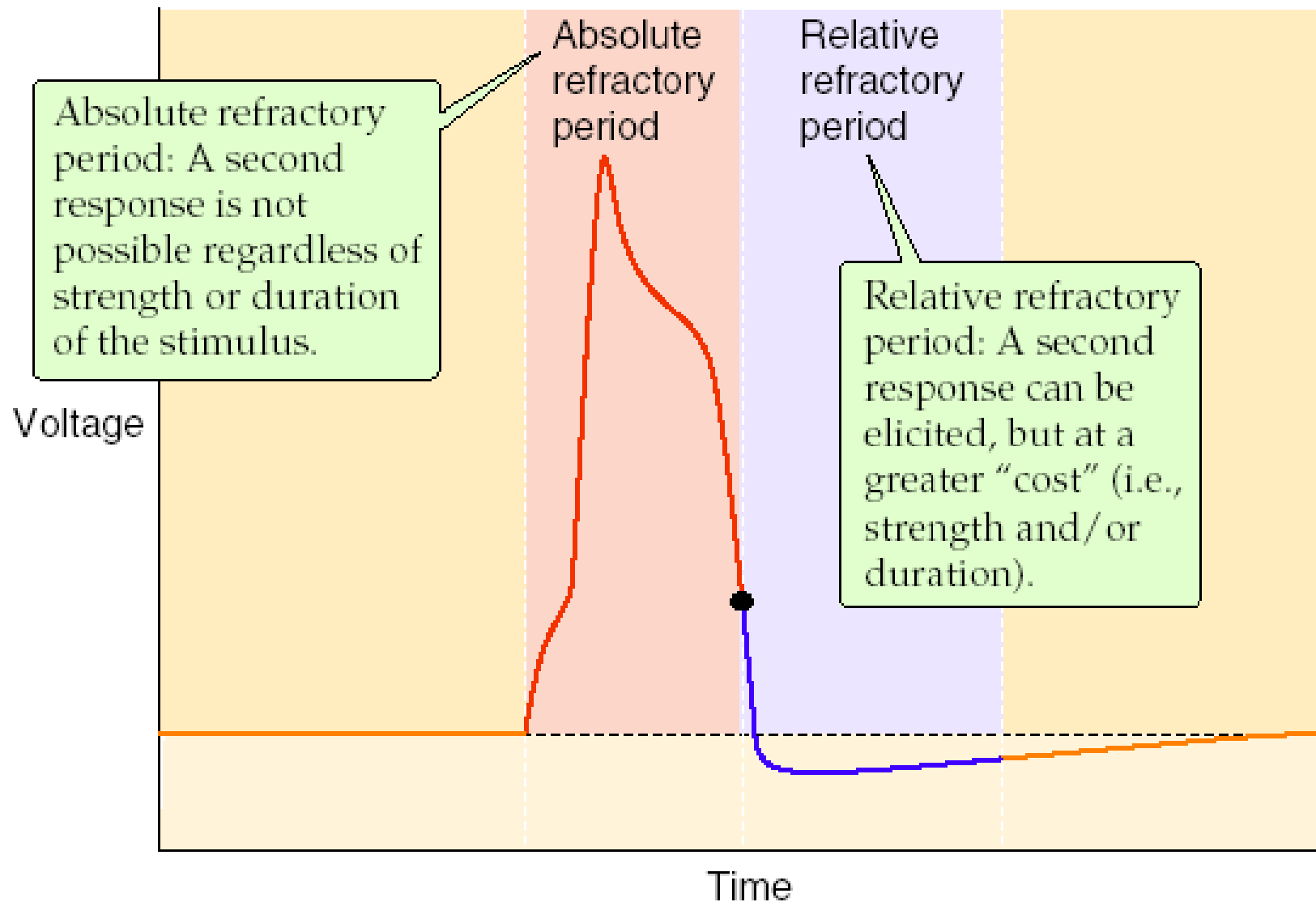
$g_i$  = conductance for ion





**B**

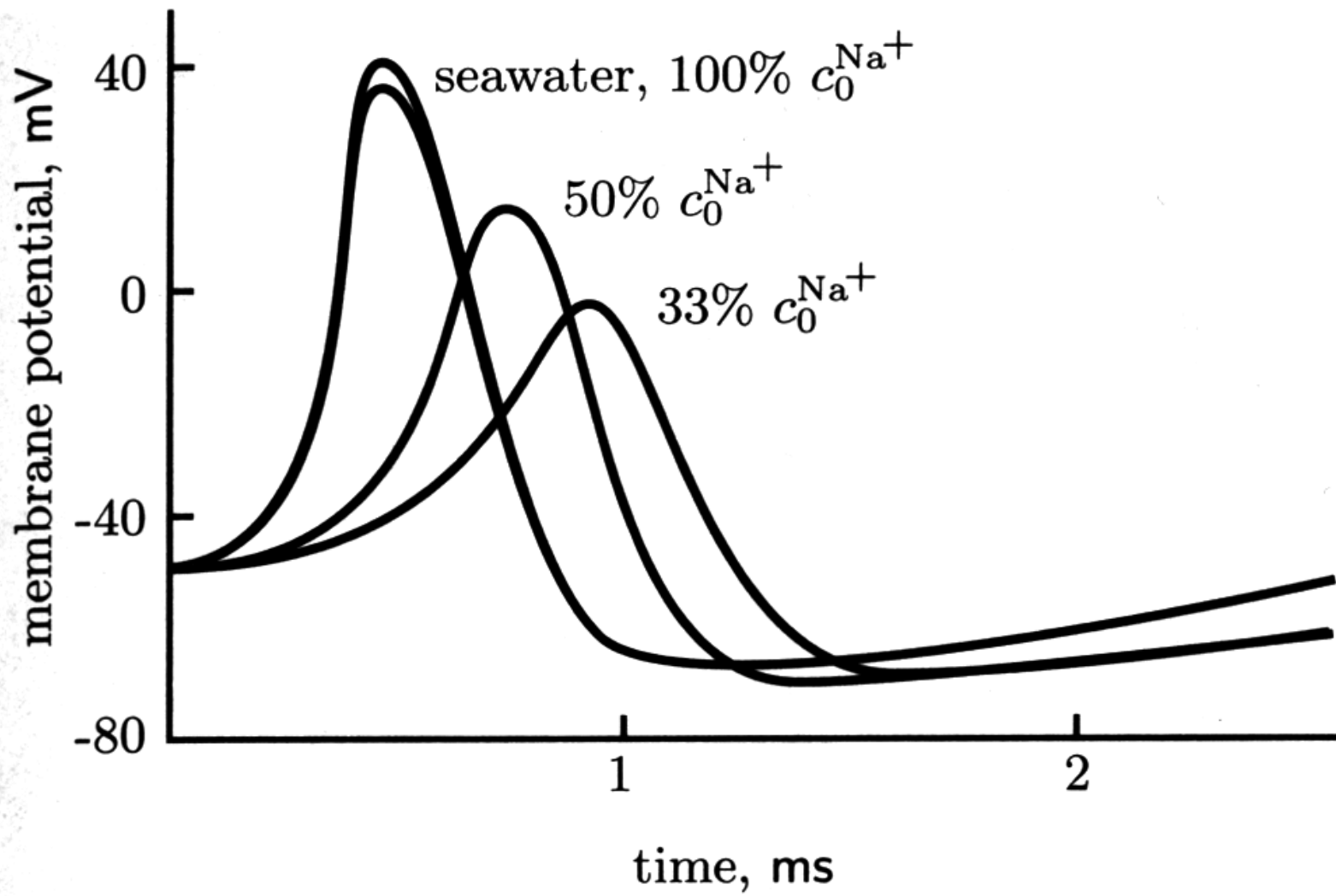




# Ion components of the action potential

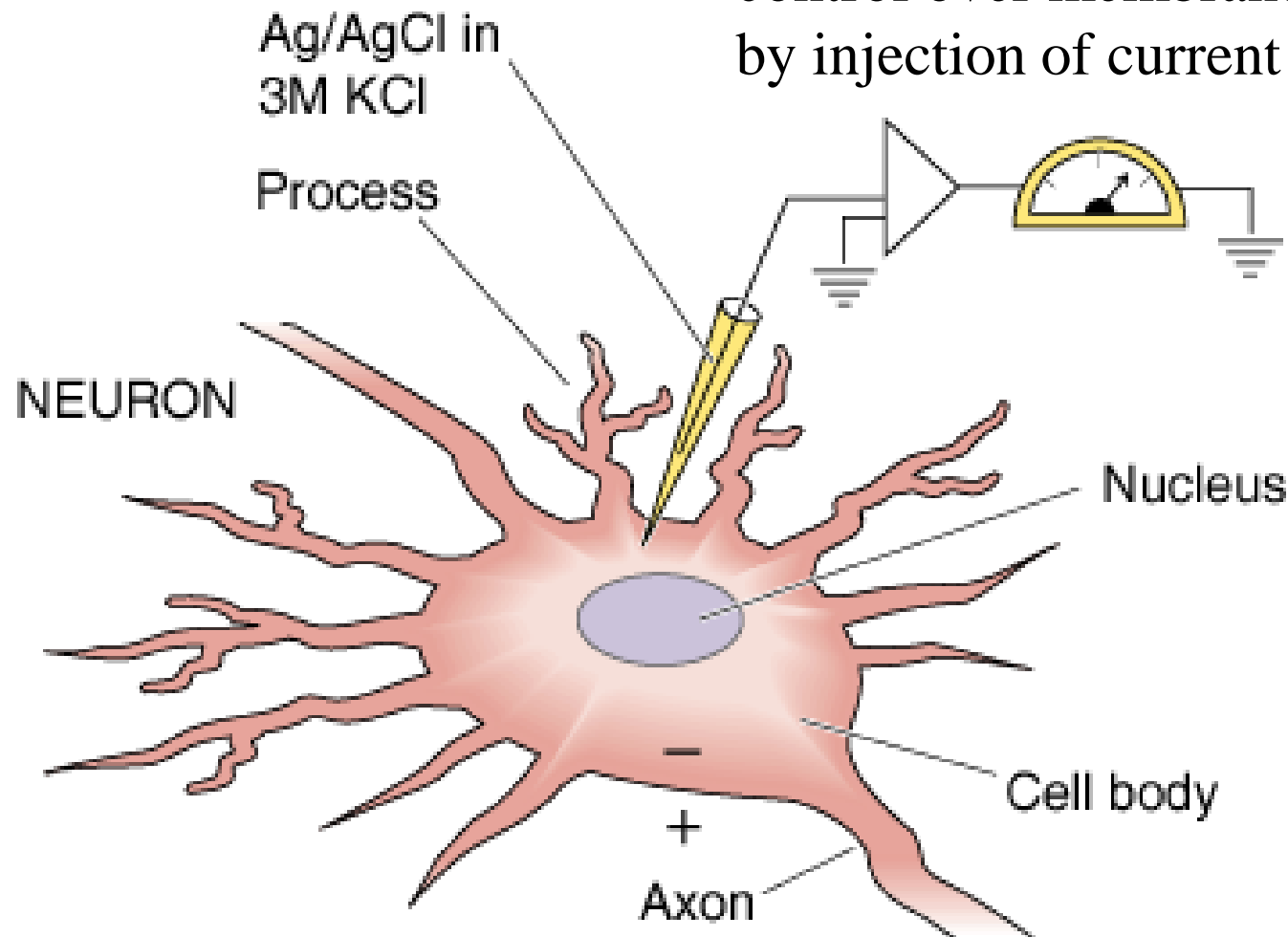
Ion	concentration (mM)		
	interstitial space	cell (“typical”)	$V^{\text{nernst}}$ (mV)
$\text{Na}^+$ , mammalian cell	145	15	+59 (37C)
$\text{K}^+$ , mammalian cell	4.5	120	-71 (37C)
$\text{Na}^+$ , squid giant axon	440	50	+54 (15C)
$\text{K}^+$ , squid giant axon	20	400	-75 (15C)

- Bernstein, **1902**.  $\text{K}^+$  conductance is key to resting potential.
- late 1930's, Cole & Curtis, and demonstrated that action potentials are associated with increased membrane conduction.
- Later, Cole & Curtis, and simultaneously by Hodgkin & Huxley, measured the transmembrane voltage, and found that it actually crossed zero, going to near +40mV, near that for Sodium
- 1940s, Hodgkin & Katz show that altering the external  $\text{Na}^+$  concentration (bringing it down from seawater, but maintaining electroneutrality), altering action potential shape (graph on next slide).



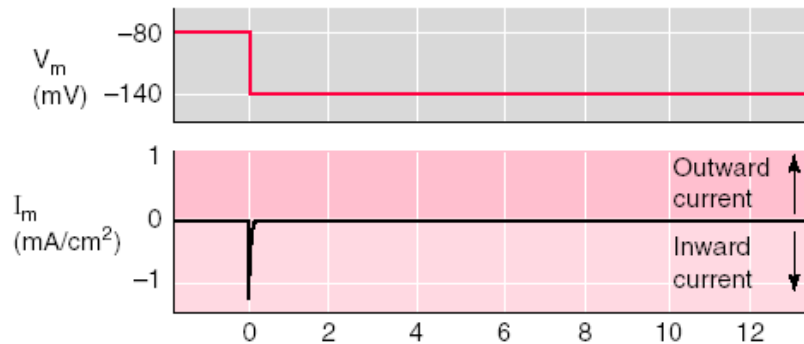
# Voltage clamp

Additional electronics allow control over membrane voltage by injection of current

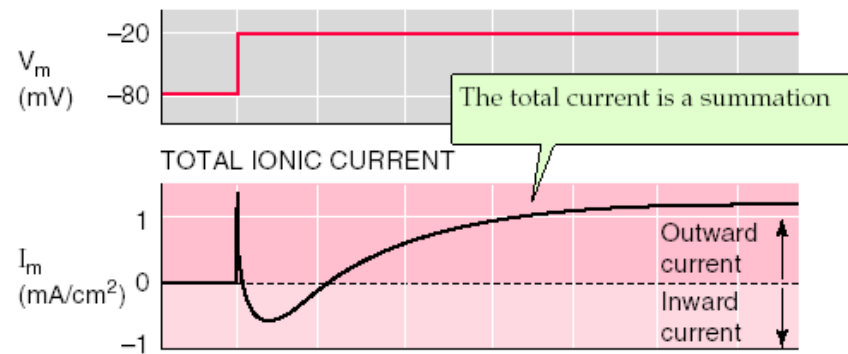




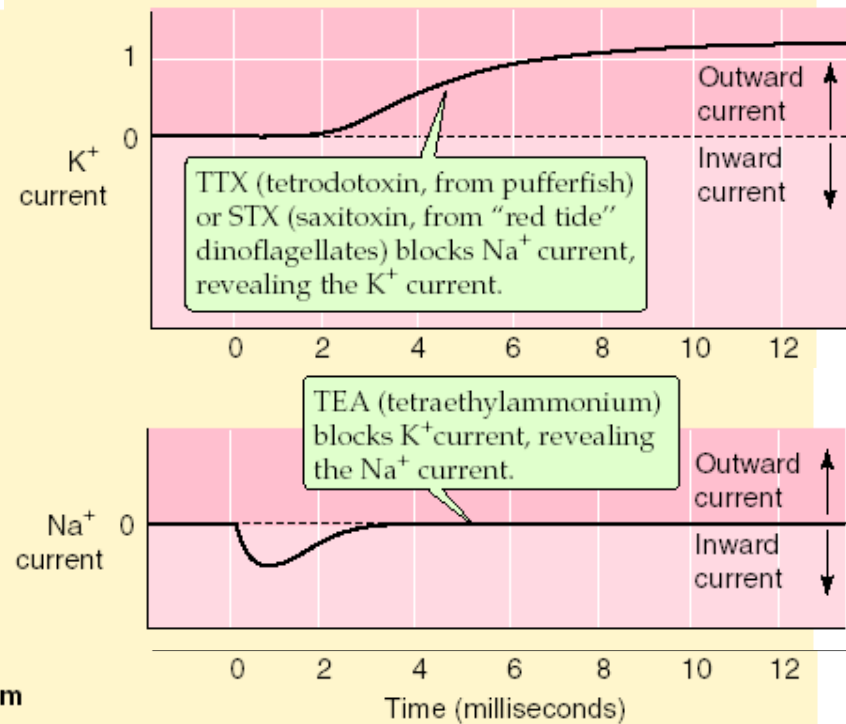
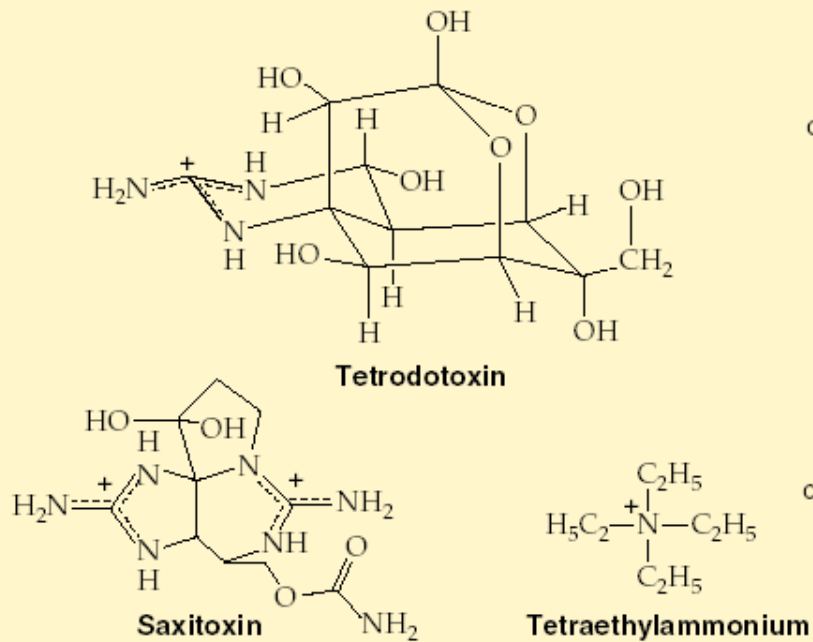
## A HYPERPOLARIZATION



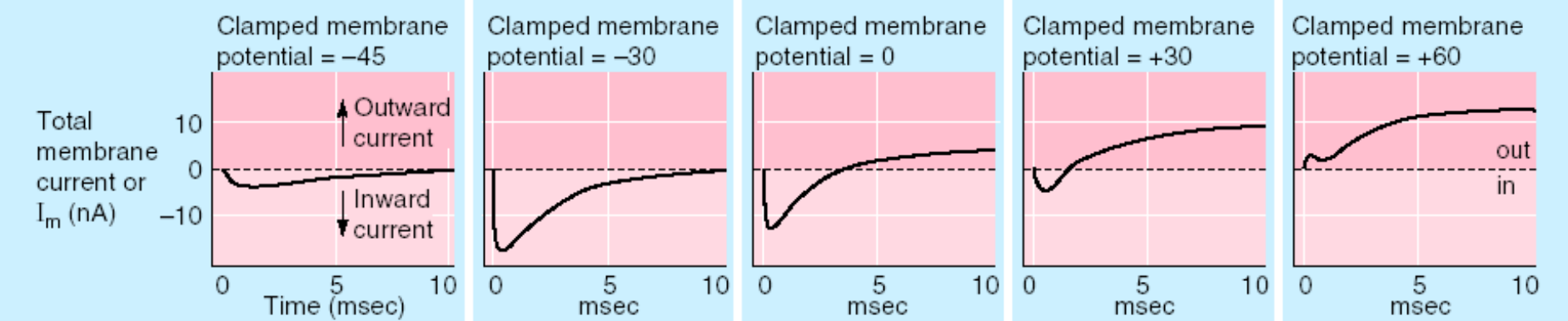
## B DEPOLARIZATION



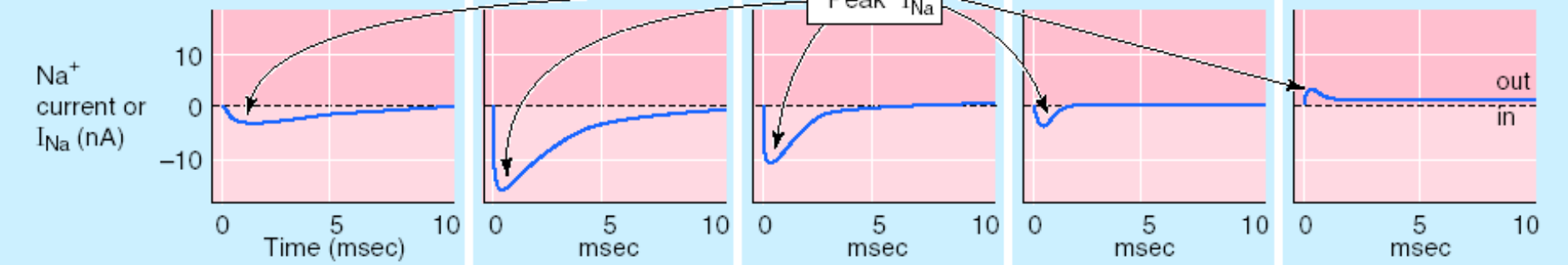
## C PHARMACOLOGICAL DISSECTION OF CURRENTS



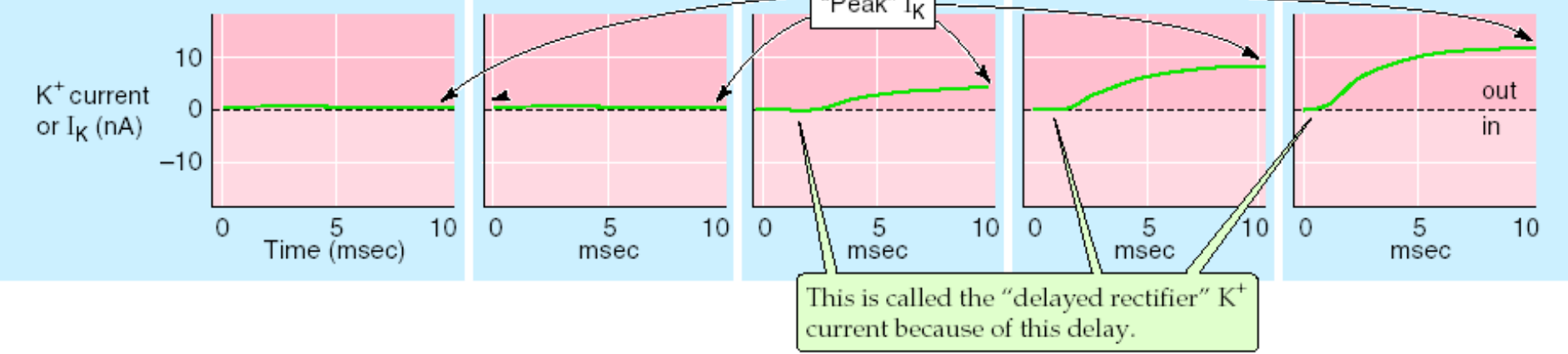
**A TOTAL IONIC CURRENT**



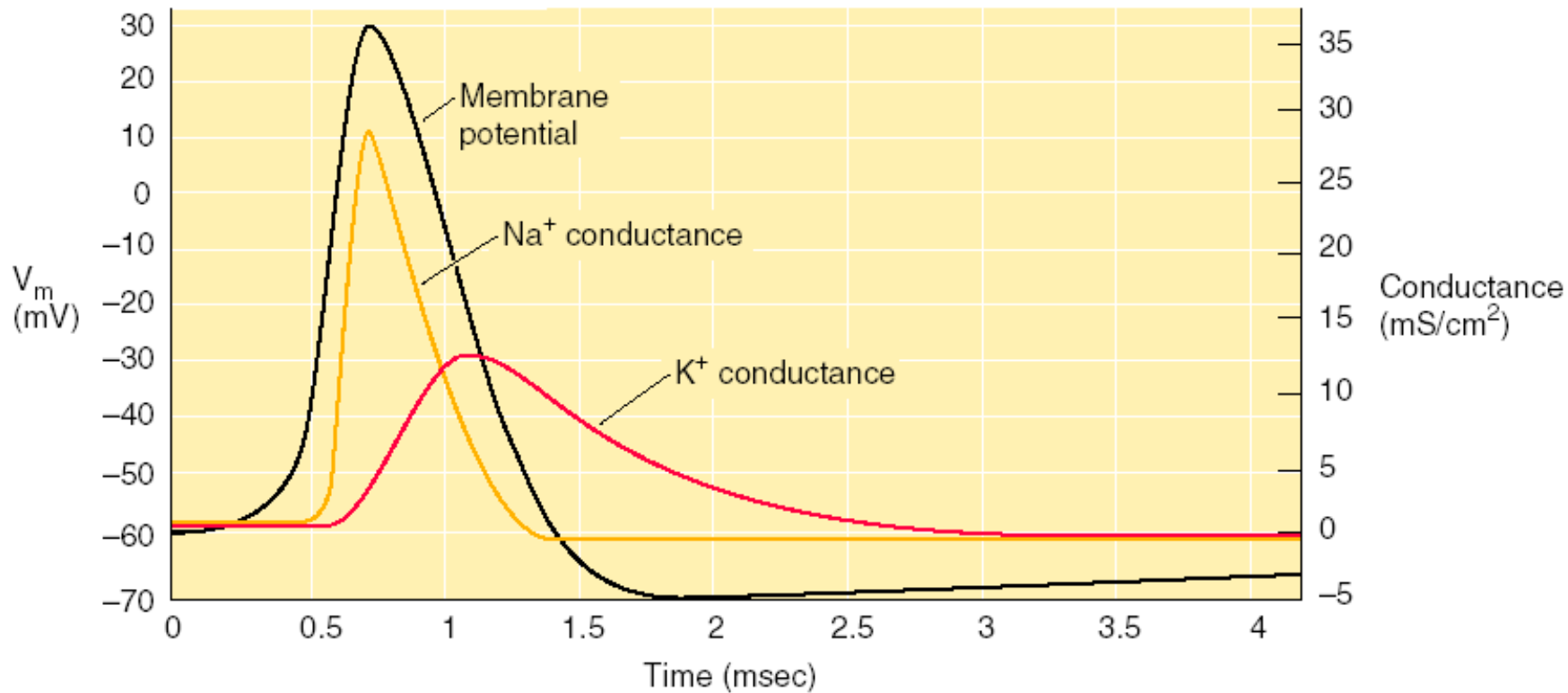
**B  $\text{Na}^+$  CURRENT OBTAINED IN 6 mM TEA**



**C  $\text{K}^+$  CURRENT OBTAINED IN 300 nM TTX**

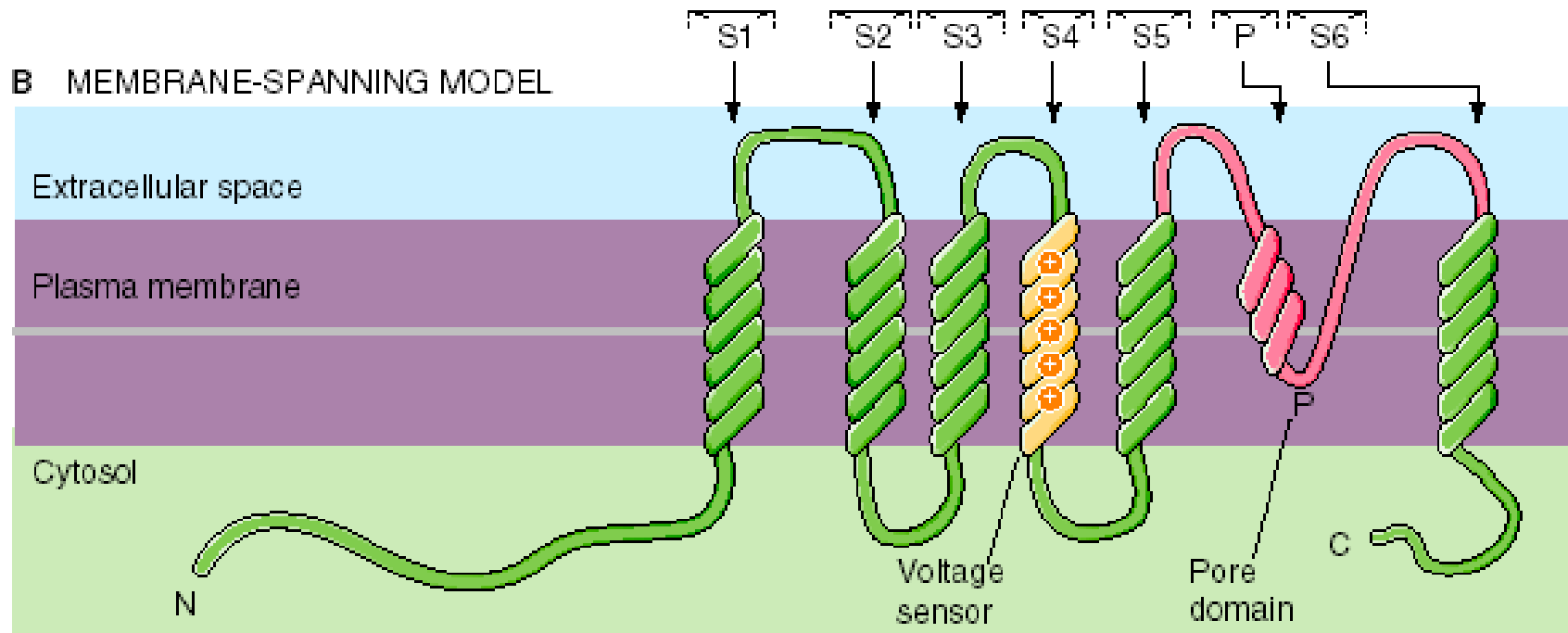


# Hodgkin & Huxley model

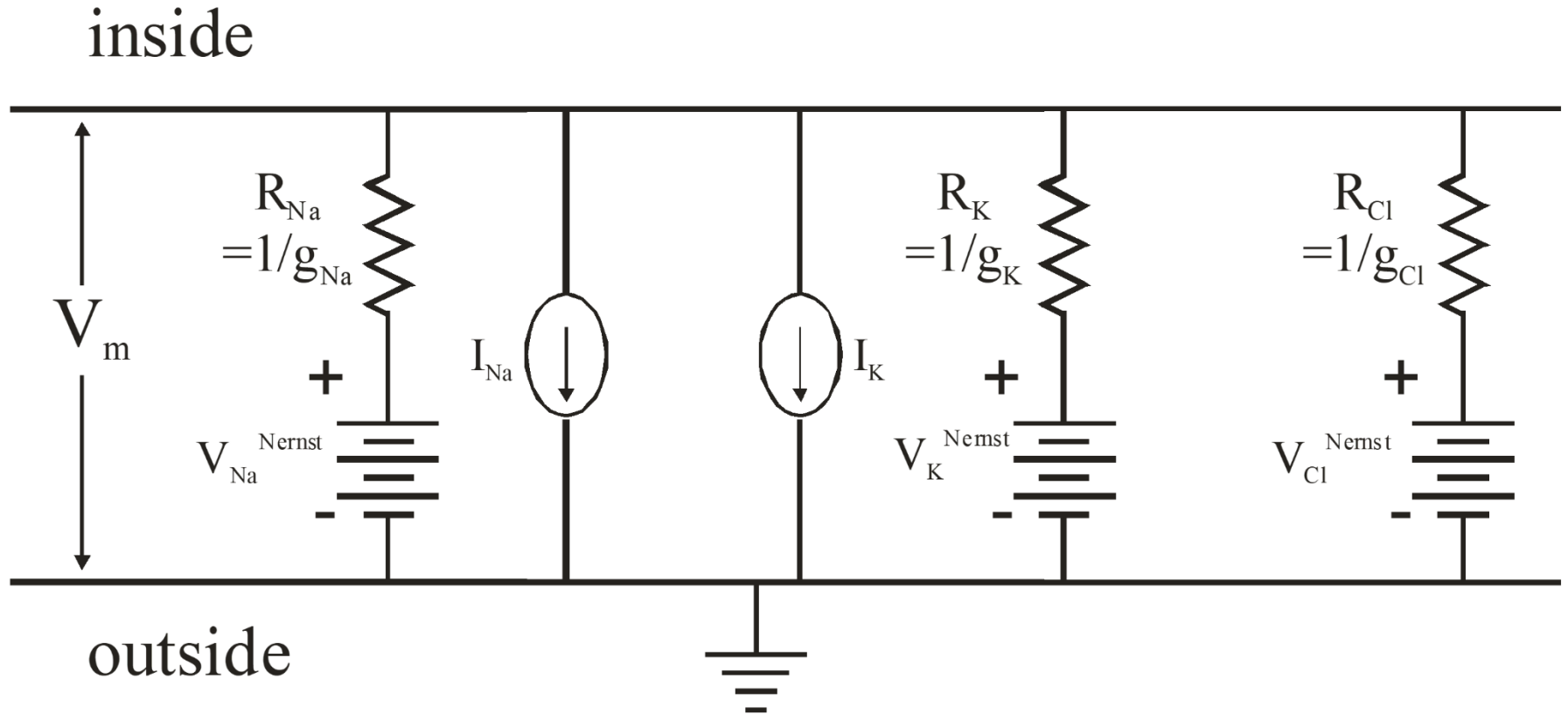


- Two channel systems, which add to conductance of the membrane
- $\text{Na}^+$  channel
  - voltage sensitive, fast opening, self-closing
- $\text{K}^+$  channel
  - voltage sensitive, slow opening v

# Voltage-sensitive channels



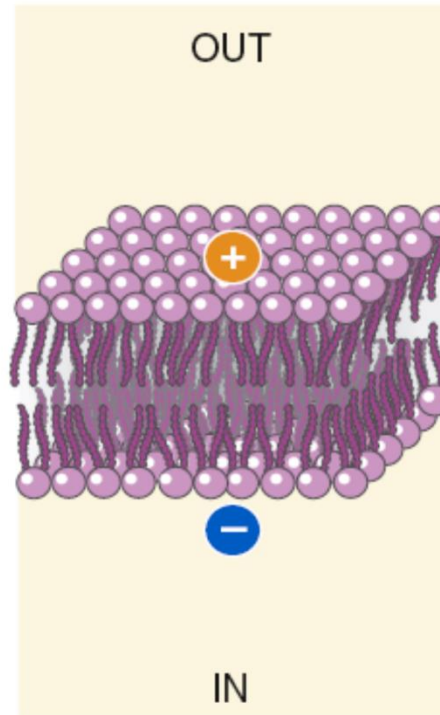
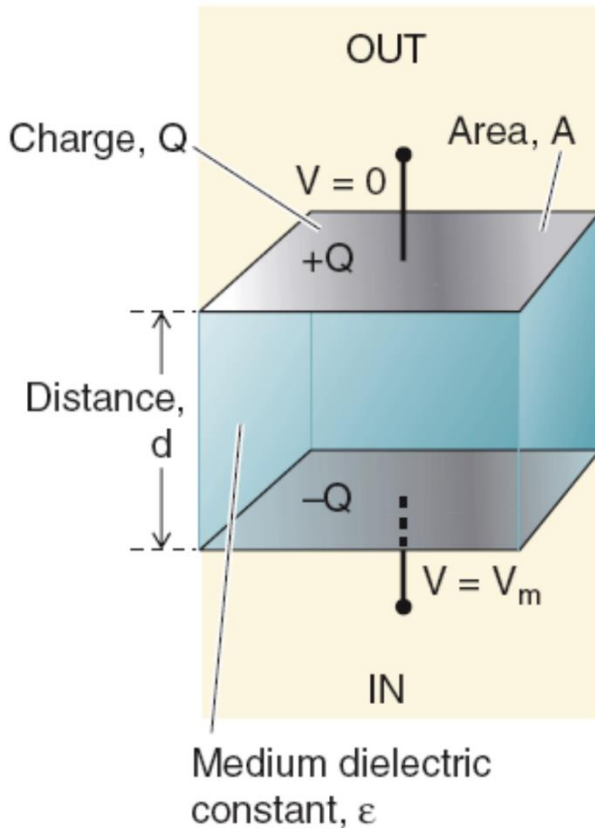
# Time dependence of membrane voltage



# Time dependence of membrane voltage

C PARALLEL-PLATE CAPACITOR

LIPID MEMBRANE



$$C = \epsilon_0 * \epsilon * A / d, \text{ or } c = \epsilon_0 * \epsilon / d$$

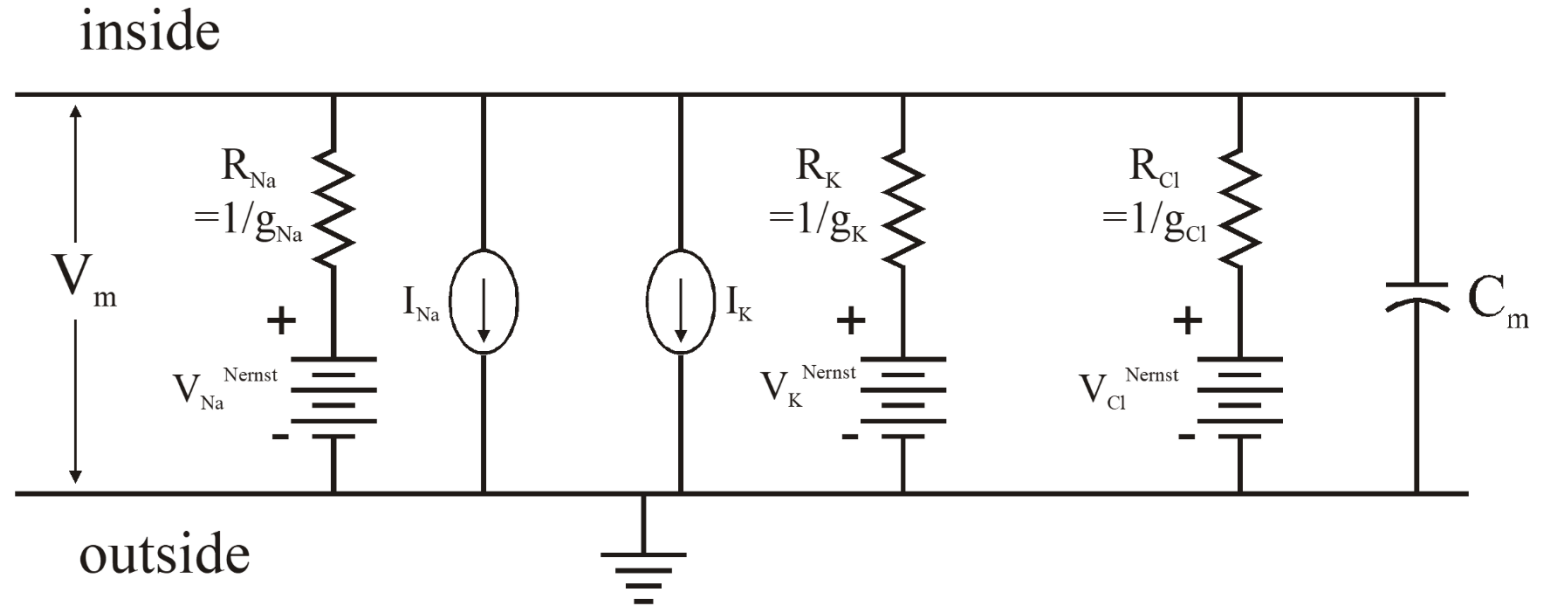
$\epsilon_0$  = permittivity constant of space  
 $\epsilon_0 = 8.854 \times 10^{-12} \text{ C}^2 / (\text{N} * \text{m}^2)$

$$\epsilon_{\text{lipid}} = 5$$

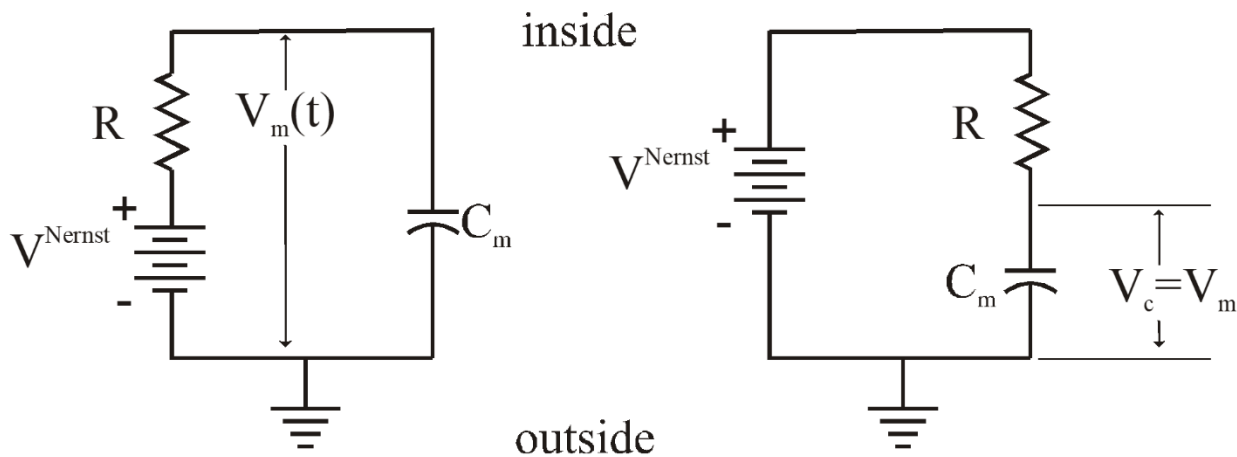
$$d \sim 5 \text{ nm}$$

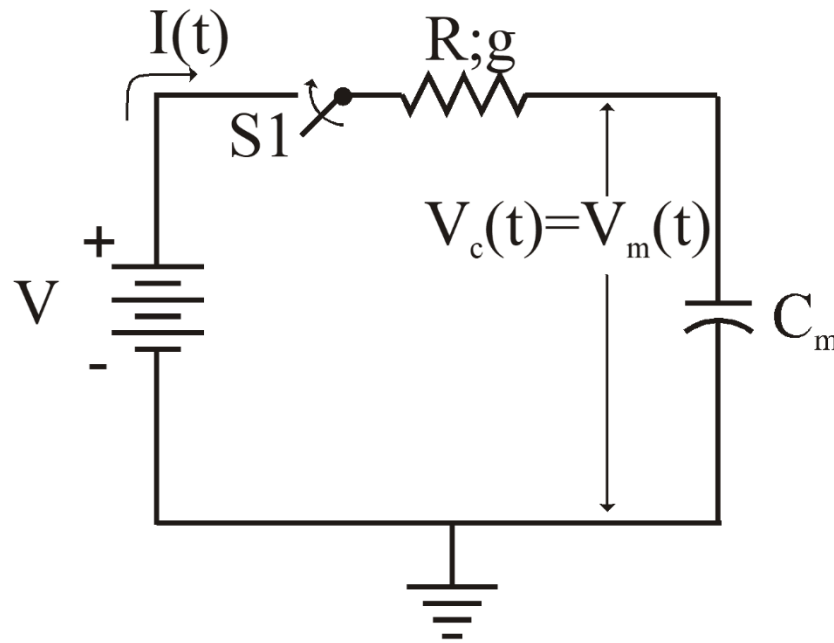
$$C = 8.85 \times 10^{-2} \text{ F/m}^2 \sim 1 \mu\text{F/cm}^2$$

# Time dependence of membrane voltage



Reduce this circuit to





- at time 0, membrane voltage is  $V_0$
- at time 0, the switch is closed, the potential “ $V$ ” is applied
- How does this system respond?

$$I(t) = g[V - V_m(t)] \text{; resistor}$$

$$I(t) = C_m \frac{dV_m(t)}{dt} \text{; capacitor}$$



$$\frac{dV_m(t)}{dt} = \frac{g}{C_m} [V - V_m(t)]$$

And now, using  $V'(t) = V_m(t) - V$ ,

$$\frac{dV'(t)}{dt} = -\frac{g}{C_m} V'(t)$$

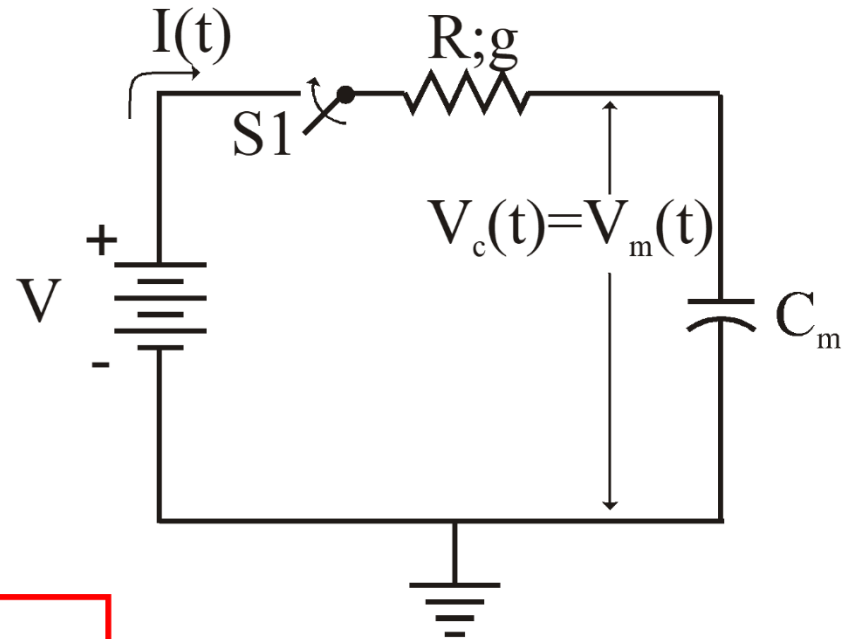
With a solution

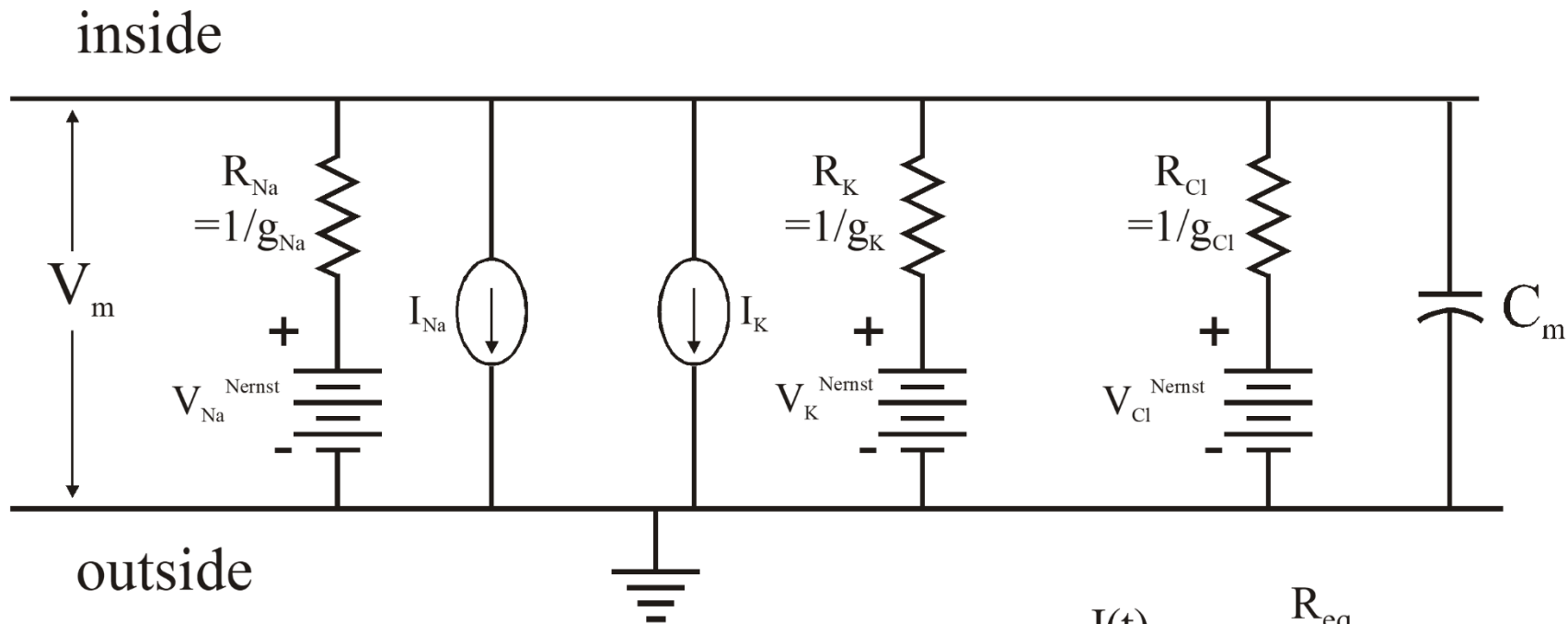
$$V'(t) = A \exp\left(-\frac{g}{C_m} t\right)$$

Using  $V_m(0) = V_0$

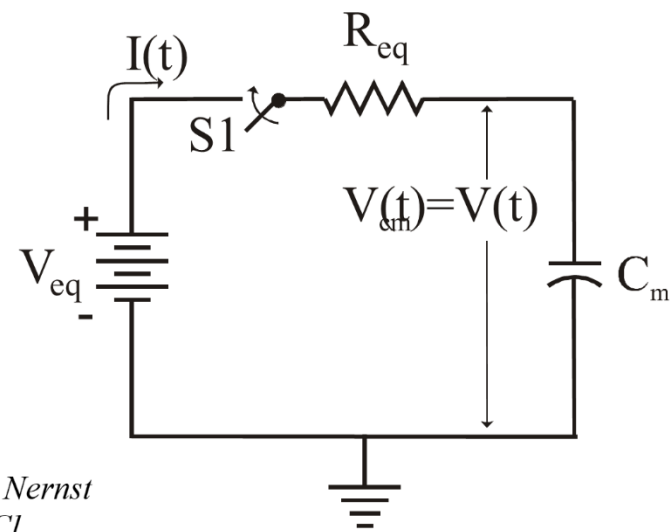
$$V_m(t) = (V_0 - V) * \exp\left(-\frac{g}{C_m} t\right) + V$$

Time constant =  $\tau = C_m/g$





$$R_{eq} = \left( \frac{1}{R_{Na}} + \frac{1}{R_K} + \frac{1}{R_{Cl}} \right)^{-1}$$



$$V_{eq}^{Nernst} = \frac{-I_{Na} - I_K + g_{Na}V_{Na}^{Nernst} + g_KV_K^{Nernst} + g_{Cl}V_{Cl}^{Nernst}}{g_{Na} + g_K + g_{Cl}}$$

Ion	concentration (mM)		
	outside	inside	$V^{\text{ernst}}$ (mV)
$\text{Na}^+$	440	50	+54
$\text{K}^+$	20	400	-75
$\text{Cl}^-$	560	52	-59

- $\text{Na}^+$  conductance, peak, action potential, squid axon:  $27 \text{ mS/cm}^2$
- $\text{K}^+$  conductance, peak, action potential, squid axon:  $12 \text{ mS/cm}^2$
- $\text{Na}^+$  conductance, resting, squid axon:  $0.1 \text{ mS/cm}^2 = 100 \text{ }\mu\text{S/cm}^2$
- $\text{K}^+$  conductance, resting, squid axon:  $1.5 \text{ mS/cm}^2$
- $\text{Cl}^-$  conductance, squid axon:  $.8 \text{ mS/cm}^2$

# resting

$$V_R = \frac{3V_{K^+}^{\text{Nernst}} g_{K^+} + 2V_{Na^+}^{\text{Nernst}} g_{Na^+}}{(2g_{Na^+} + 3g_{K^+})}$$

$$\Delta V = -70 \text{ mV}$$

# open Na<sup>+</sup> channels

- $g_{\text{Na}} = 27 \text{ mS/cm}^2$
- $g_{\text{K}} = 1.5 \text{ mS/cm}^2$
- $g_{\text{Cl}} = 0.8 \text{ mS/cm}^2$
- Pump-leak  $\Rightarrow 44 \text{ mV}$

Consider a 500  $\mu\text{m}$  diameter axon, take a 1  $\mu\text{m}$  length

$$\text{Area} = \pi * 500 \mu\text{m} * 1 \mu\text{m} = 1570 \mu\text{m}^2$$

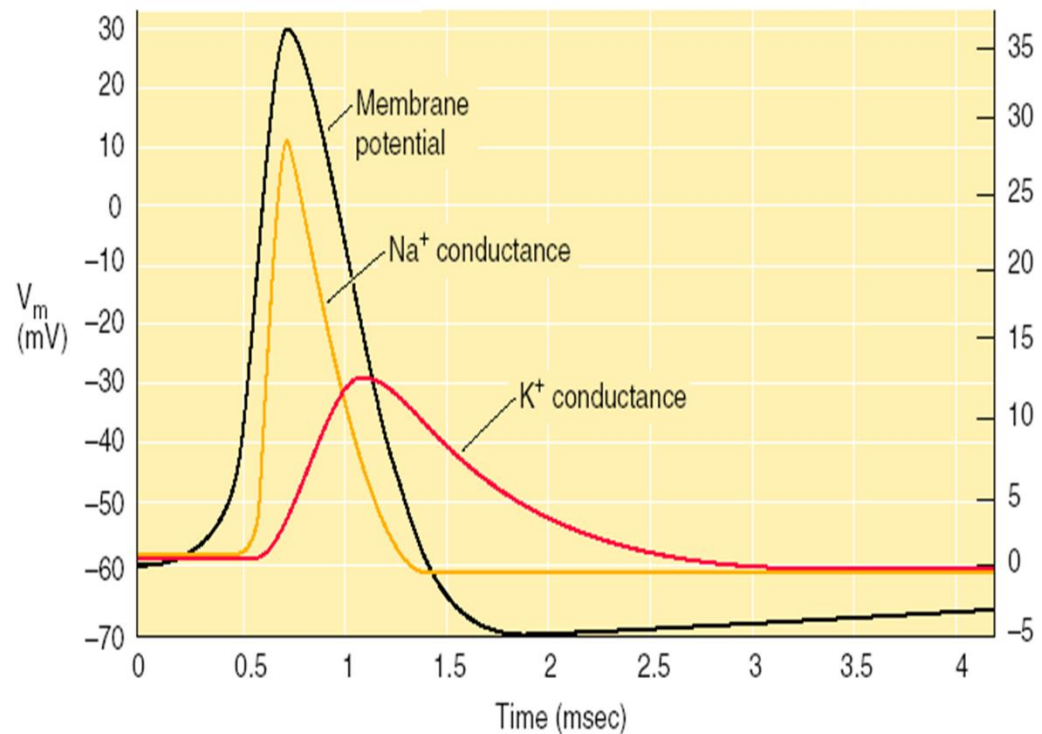
$$\text{Capacitance} = 1 \mu\text{F/cm}^2 * 1570 \mu\text{m}^2 * (1\text{E-}8 \text{ cm}^2/\mu\text{m}^2) = 1.6\text{E-}11 \text{ Farad}$$

$$\text{Resistance for this patch} = 1/(g_{\text{Na,AP}} * 1570 \mu\text{m}^2) = 1/(4.2\text{E-}7\text{S}) = 2.36 \text{ M}\Omega$$

$$\text{Time constant} = 3.7\text{E-}5 \text{ seconds} \sim 35 \mu\text{s}.$$

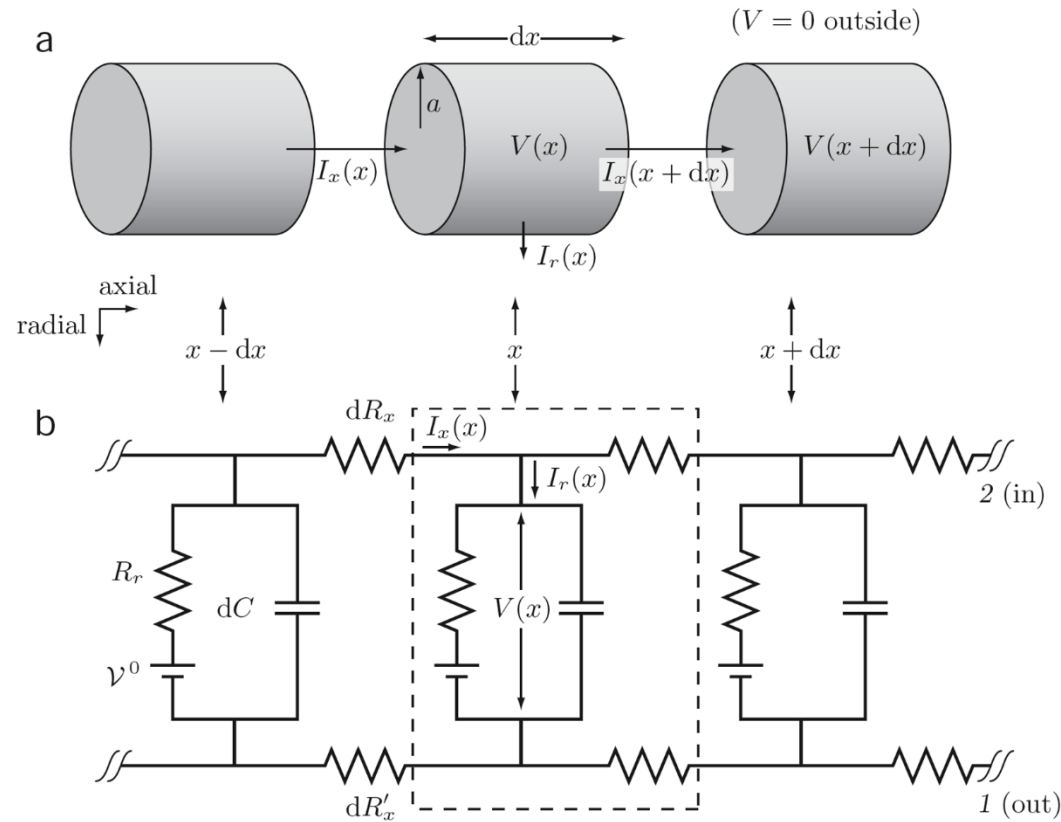
# repolarization

- $g_{\text{Na}} = 7 \text{ mS/cm}^2$
- $g_{\text{K}} = 12 \text{ mS/cm}^2$
- $g_{\text{Cl}} = 0.8 \text{ mS/cm}^2$



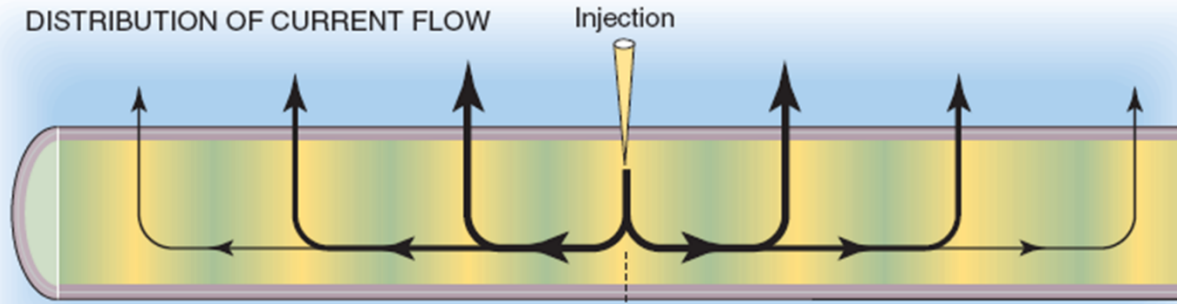
time constant =  $53 \mu\text{s}$

# Cable equation – linear solution

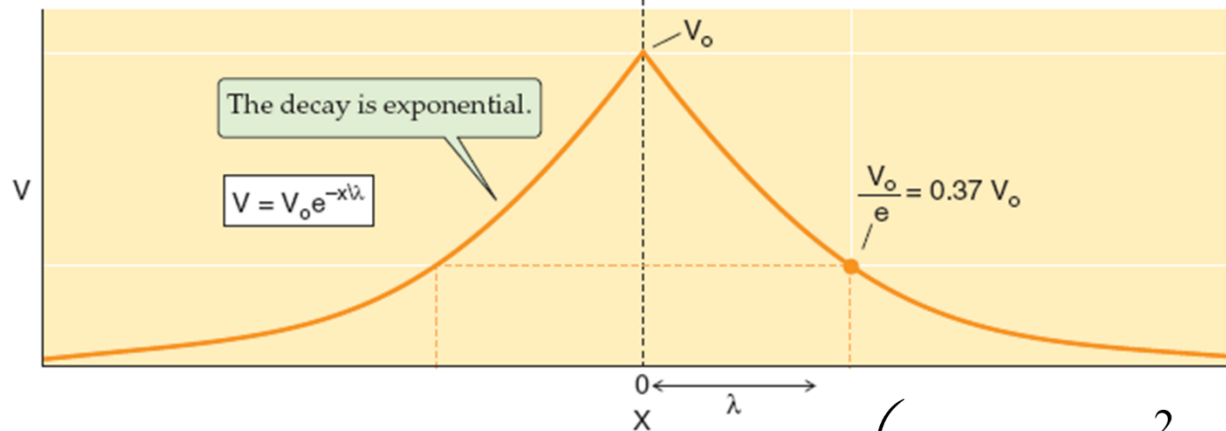


- Treat axon membrane as chain of cylinders, each with radial and axial components
- Extend this concept to create a continuum of distributed resistors and capacitance
- Typically, solve for voltages and currents as function of position

B DISTRIBUTION OF CURRENT FLOW



C VOLTAGE DECAY



$$v(x, t) = C * \exp(-t / \tau) * t^{-1/2} * \exp\left(-\frac{x^2}{\left(4 * t * \lambda^2 / \tau\right)}\right)$$

$\tau = C_m * R_m$ ; time constant

$R_m$  = membrane resistance

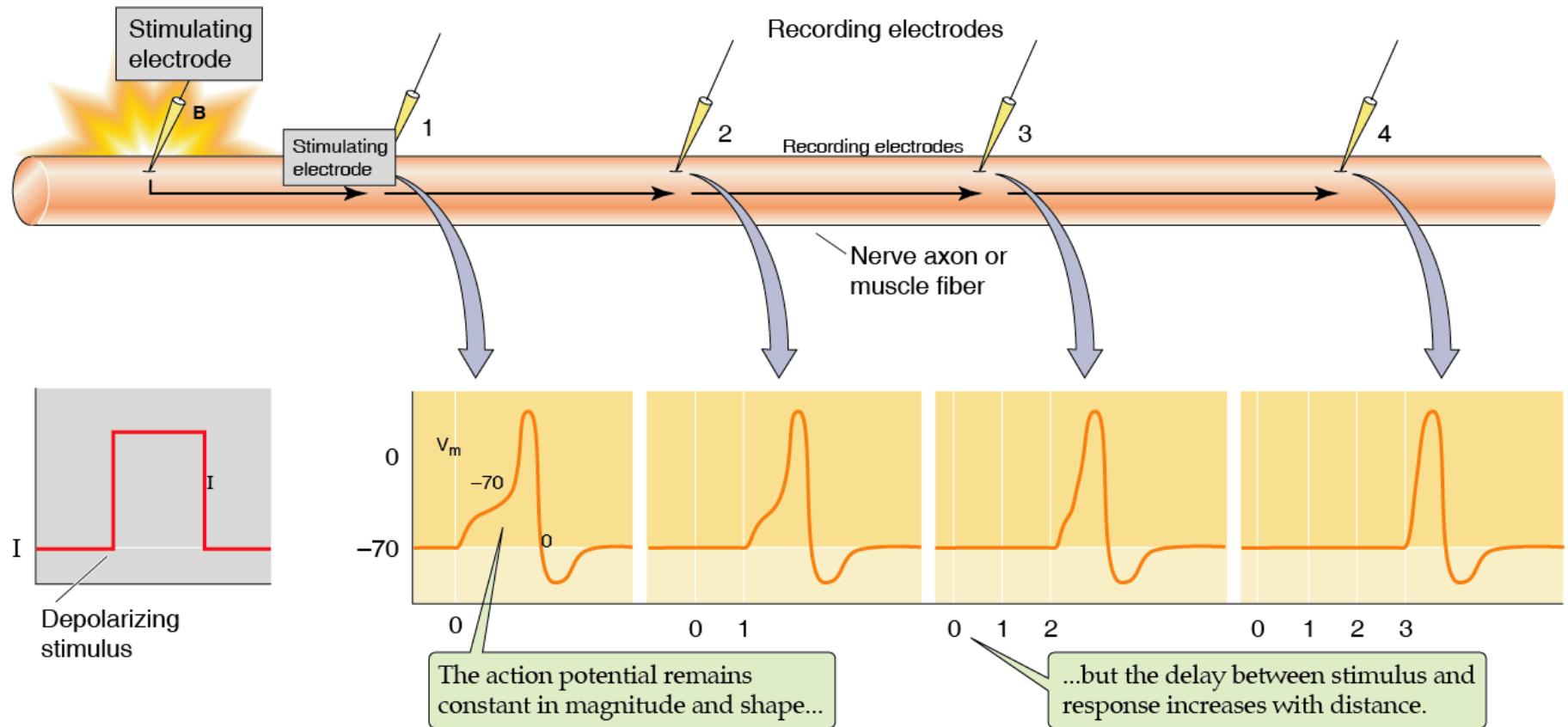
$\lambda$  = 0.1 mm to 10's of mm  
under typical conditions

$\lambda = \text{sqrt}(a * R_m / (2 * R_i))$ ; length constant

$R_i$  internal resistance,  $a$  = radius

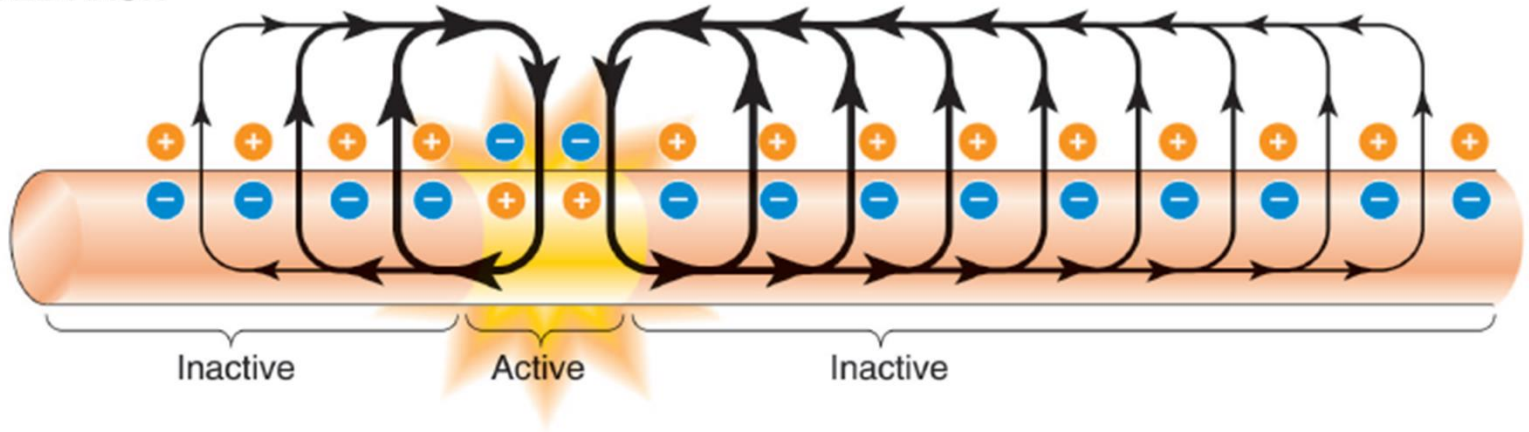


# Traveling action potentials

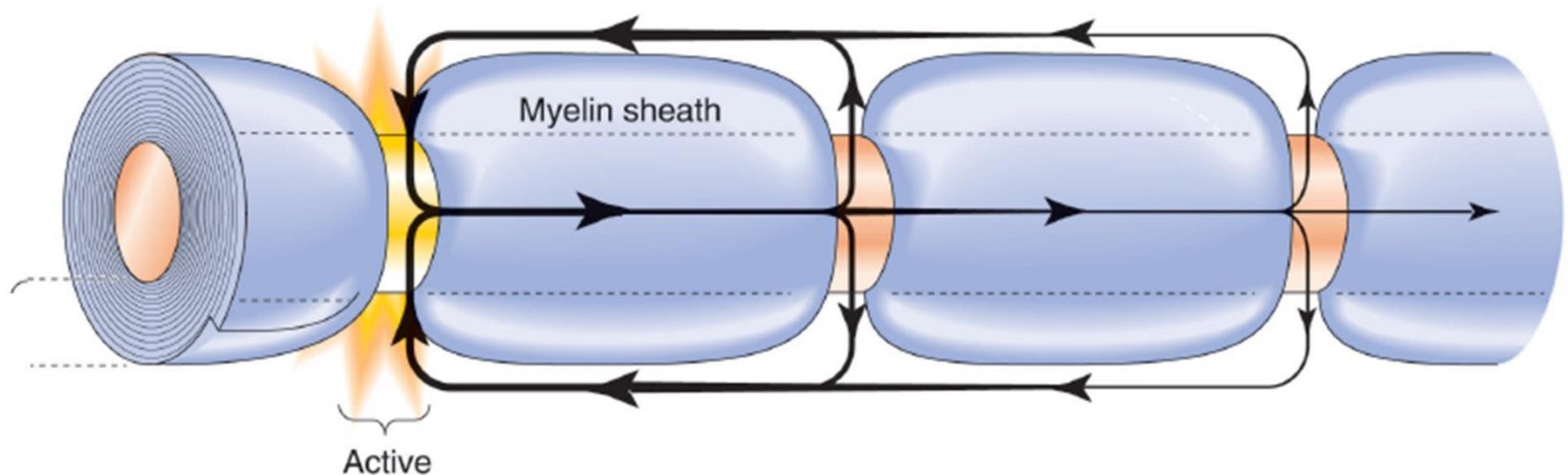


# initiation of action potentials

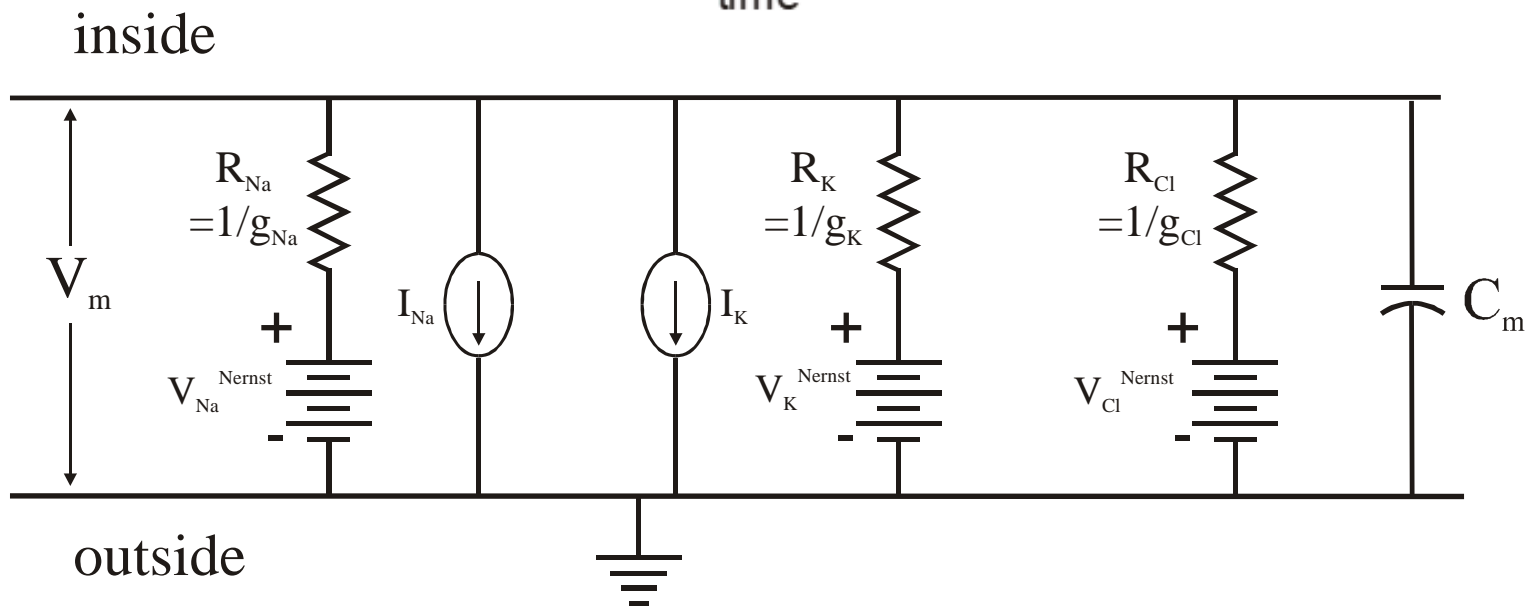
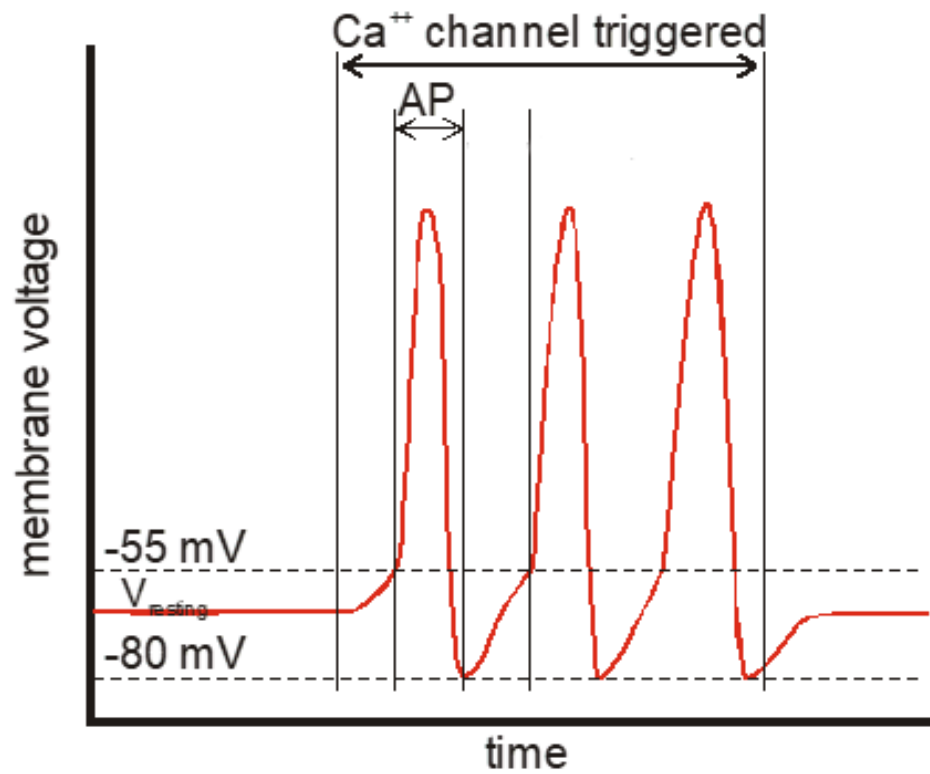
**A** UNMYELINATED AXON



**B** MYELINATED AXON

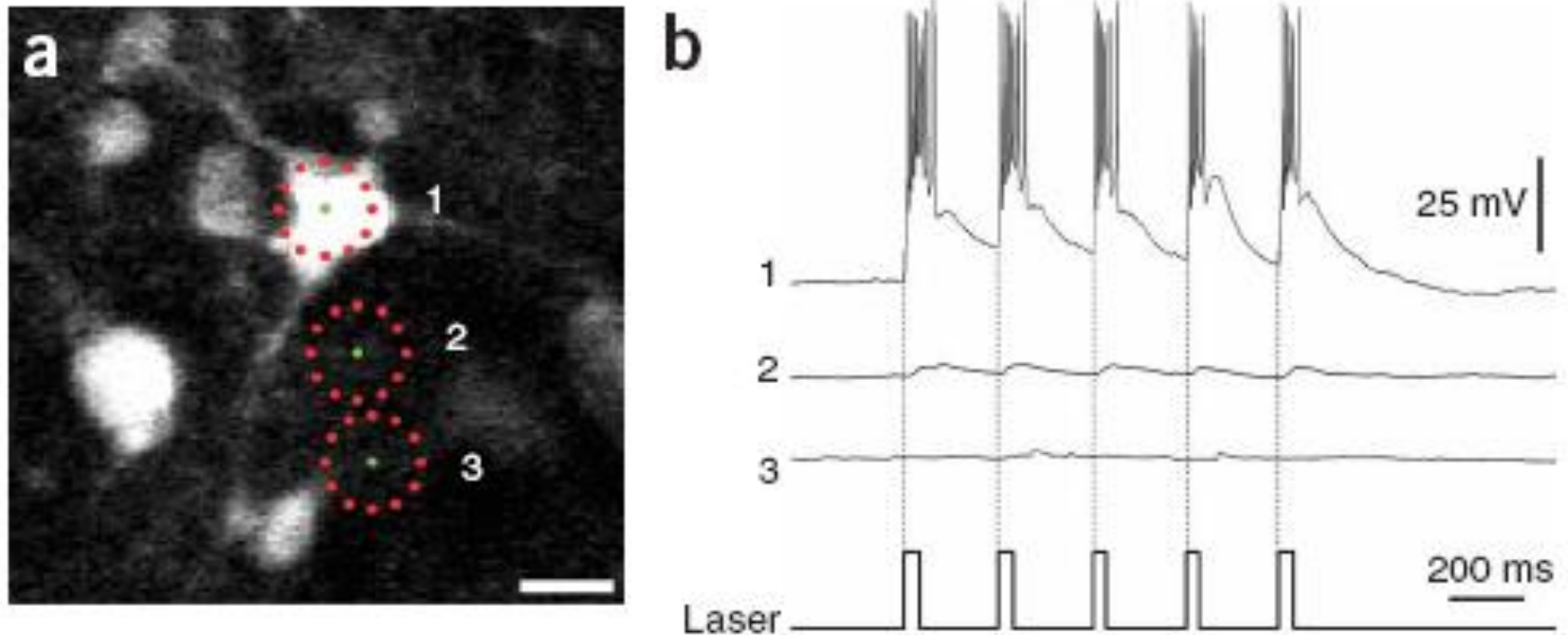


Myelination enhances transmission by reducing capacitance and increasing membrane resistance



## Optic-driven stimulation in slices

Nikolonko, Poskanzer, & Yuste, *Nat Methods*, 4:943 (2007)

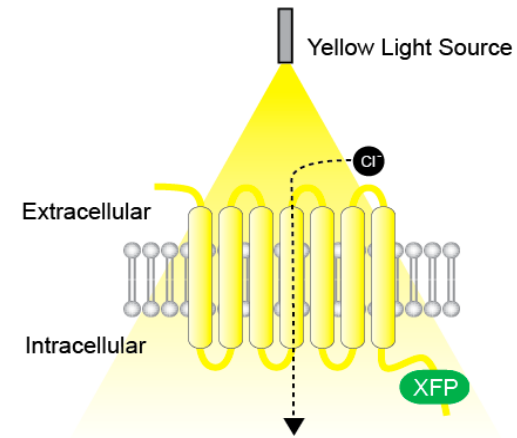
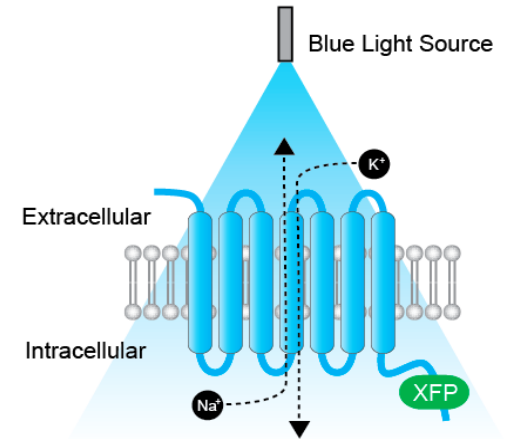


- Laser-induced uncaging of glutamate

# Optogenetics. Deisseroth, K., *Sci Am* **303**:48-55 (2010)



Channelrhodopsin-2  
nonspecific cation channel, depolarize



Halorhodopsin  
chloride pump, hyperpolarize

